Science Advances NAAAS

Supplementary Materials for

A computational mechanism of cue-stimulus integration for pain in the brain

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Sci. Adv. **10**, eado8230 (2024) DOI: 10.1126/sciadv.ado8230

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Figs. S1 to S10 Table S1 References

Fig. S1. Calculating encoding performances. Calculating encoding performance. Group average FIR time-series data projected onto cue and stimulus subspaces create neural trajectories, represented by colored lines. We selected the two most distant conditions among trajectories at single time points (yellow dots with black outlines) and then drew the line that connects the two. We then projected the same time point (white dots with black outlines) of other trajectories onto the line, resulting in a one-dimensional vector (yellow dots) that encoded distance information between trajectories. This is what we referred to as inter-trajectory distances, which we used to calculate encoding performances and reconstruct pain ratings.

Fig. S2. Principal gradient scores from the resting-state fMRI data of the participants in this study. The figure shows voxel-wise principal gradient scores from the first gradient of the whole-brain resting-state fMRI ($N = 56$). We used diffusion embedding implemented in the BrainSpace Toolbox (*99*) for the calculation of the gradient. The gradient scores for each network were obtained using the network mask employed in the current study. Resting-state data were up-sampled to 3 mm for the gradient calculation.

Fig. S3. The variance explained by the principal components constituting the cue and stimulus subspaces. The upper panel displays the variance explained by principal components constituting the cue subspace, while the lower panel displays the variance explained by principal components constituting the stimulus subspace. Dashed lines represent the number of principal components explaining 70% variance for each network. We used 20 dimensions for all networks to control for differences arising from the different number of dimensions. With 20 dimensions, the percentage of explained variance in the cue subspace ranges from 70% in the limbic network to 97% in the visual network. In the stimulus subspace, it ranges from 74% in the limbic network to 94% in the visual network.

Fig. S4. Effect sizes of large-scale networks. (A) Effect sizes, calculated as the subtraction of null encoding performances from the actual encoding performances, for all seven networks. The green plots show effect sizes in the cue subspace, and the orange plots show effect sizes of the stimulus subspace. **(B)** Averages of cue and stimulus effect sizes across networks. The left panel displays the effect sizes for the cue subspace, while the right panel illustrates the effect sizes of the stimulus subspace. **** $p < 0.0001$, two-tailed, paired *t*-test.

Fig. S5. Encoding performances and neural trajectories of the dorsal attention (dAttention) and ventral attention (vAttention) networks. (A-B) Encoding performances of the dAttention **(A)** and vAttention networks **(B)**. The encoding performances of the stimulus were significantly larger than those of the cue in both dAttention network ($t_{48} = 5.626$, $p = 9.286$ e-7, two-tailed, paired *t*-test) and vAttention network ($t_{48} = 2.628$, $p = 0.012$, two-tailed, paired *t*-test). The layout is the same as Figs. 4A-C, D**.** The encoding performances were based on the actual versus null subspaces of the dAttention **(C)** and vAttention networks **(D)**. **(E-F)** Neural trajectories of the dAttention **(E)** and vAttention networks **(F)**. The trajectories were smoothed with a Gaussian kernel (standard deviation: 3 TRs) for visualization purposes, but the unsmoothed trajectories were employed for the actual analysis. The layout is the same as **Figs. 4G-I**. $p < 0.05$; **** $p <$ 0.0001, two-tailed, paired *t*-test.

Fig. S6. Relationship between effect sizes and the network sizes. Network-level statistics cue effects, stimulus effects, and reconstruction fits—were compared with their number of voxels within each network. We calculated Spearman's rank correlation between the temporal averages of these statistics and the number of voxels for each network to account for their different scales. From the left panel to the right panel, each panel shows the number of voxels on the x-axis and cue effects, stimulus effects, and reconstruction fits on the y-axis, respectively, all of which showed no significant correlation. (cue effects: $r_s = -0.143$, $p = 0.783$; stimulus effects: $r_s = -0.179$, $p = 0.713$; reconstruction fits: $r_s = -0.071$, $p = 0.906$; two-tailed, Spearman's rank correlation)

Fig. S7. Reconstructed pain ratings using a different number of principal components

(PCs). (A-G) Comparison of the actual and reconstructed pain ratings from each of the 7 largescale networks. In all figures, the left panel shows reconstructed pain ratings from neural trajectories within cue and stimulus subspaces of 10 PCs. The middle and the right panels show the results using 20 PCs and 30 PCs, respectively. The colored (red, blue, and gray) lines indicate the reconstructed pain ratings, while the black lines indicate average pain ratings across participants. Both metrics are normalized for comparison between the two. **(H)** Reconstruction fits from each network using a different number of PCs. These were calculated as *R*-squared values of the reconstructed ratings for every time point. Results obtained using 20 PCs are also included in the main figures and results. In all cases, reconstruction fits were significant for the limbic, default mode, and vAttention networks. In the limbic network, using 10 PCs, md (median) = 0.883, *z* = 6.088, *p* = 5.236 e-10; 30 PCs, md = 0.905, *z* = 6.088, *p* = 5.236 e-10. In the default network, using 10 PCs, md = 0.752 , $z = 2.944$, $p = 0.002$; 30 PCs, md = 0.806 , $z =$ 3.342, $p = 4$ e-4. In the vAttention network, using 10 PCs, md = 0.852, $z = 2.139$, $p = 0.016$; 30 PCs, $md = 0.856$, $z = 2.586$, $p = 0.005$. Note that using 30 PCs showed significant reconstruction fit also in the frontoparietal network (md = 0.506 , $z = 1.870$, $p = 0.031$). All *p* values are onetailed and from Wilcoxon signed rank test with 49 time points. Networks are aligned in a descending order of the median. The results with 20 PCs are presented as the main results and figures. p^2 < 0.05, p^* *p* < 0.01, p^* *p* < 0.001, p^* *p* < 0.0001.

Fig. S8. Results of searchlight analysis. We conducted searchlight analyses for all gray matter voxels. The spherical searchlight radius size was 5 voxels. **(A)** Voxels with significant cue (middle panel) and stimulus (lower panel) encoding performances. Significance was determined using a paired *t*-test, with $df = 48$, Bonferroni corrected $p < 0.05$. The upper panel displays the template brain, with each column corresponding to the same spatial axis as in the middle and lower panels. **(B)** Voxels with significant reconstruction fit (left panel) and the radial plot showing proportions of significant voxels within a large-scale network (right panel). Significance follows the same criterion as in **(A)**, but with a one-tailed Wilcoxon signed rank test. In the radial plot, the proportions occupied by each network were calculated as the number of occupying voxels divided by the total voxel count of the respective network.

Fig. S9. Encoding performances and reconstruction fits of large-scale networks comprising only the cerebrum. **(A)** Encoding performances of all 7 large-scale networks. The encoding performance was calculated for each time point, and the plots show the time information with the graded colors ranging from cool (early) to warm (late) colors. **(B)** Encoding performances based on the actual cue subspace versus the null subspace. **(C)** Encoding performances based on the actual stimulus subspace versus the null subspace. **(D)** The colored (red, blue, and gray) lines show the reconstructed pain ratings from distances of neural trajectories in subspaces, and black lines indicate averaged pain ratings from participants, also normalized for comparisons with the reconstructed pain ratings. The error bars indicate SEM across time. **(E)** Reconstruction fits of the large-scale networks. Reconstruction fits were calculated with *R*-squared values of the reconstructed pain rating at each time point. Networks are aligned in a descending order of the median. * *p* < 0.05, ***p* < 0.01, ****p* < 0.001, *****p* < 0.0001

Fig. S10. Residuals from multilevel GLM of behavioral data. (A) A histogram of trial-level residuals of pain ratings after accounting for the effects of cues, stimulus intensities, their interactions, and participants. **(B)** A Quantile-Quantile plot of the residuals of pain ratings. The dots indicate the residuals of single trials, and the red line represents the expected distribution if the residuals perfectly follow a normal distribution.

Table S1. Effect sizes with different numbers of principal components

	Cue						Stimulus					
Networks	NumPC 10		NumPC 20		NumPC 30		NumPC 10		NumPC 20		NumPC 30	
Visual	8.932	8.932E-12	8.243	9.466E-11	8.107	1.517E-10	5.604	002E-06	5.818	4.753E-07	5.919	3.333E-07
Somatosensory	7.473	.388E-09	7.366	2.021E-09	7.547	1.071E-09	7.533	1.125E-09	7.451	1.502E-09	7.889	3.247E-10
dAttention	5.364	2.310E-06	5.142	4.962E-06	5.098	5.772E-06	8.043	L899E-10	7.977	2.388E-10	7.944	2.678E-10
vAttention	14.979	1.013E-19	14.482	3.830E-19	15.211	5.487E-20	8.279	8.364E-11	10.211	1.273E-13	11.632	1.431E-15
Limbic	16.630	.484E-21	24.801	5.089E-29	30.604	3.810E-33	9.546	1.132E-12	13.718	3.148E-18	18.528	1.646E-23
Frontoparietal	6.551	3.598E-08	7.322	2.362E-09	7.963	2.503E-10	8.483	4.136E-11	8.220	1.026E-10	8.510	3.780E-11
Default	6.589	3.144E-08	7.126	4.717E-09	8.192	1.130E-10	7.663	7.145E-10	9.135	4.495E-12	9.826	4.483E-13

Note. The table shows *t*-values and *p* values of cue and stimulus effect sizes from paired *t*-test (*df* = 48, two-tailed). We calculated cue and stimulus effect sizes in all 7 large-scale networks using different numbers of principal components (denoted as NumPC). The results remained significant regardless of the number of PCs constituting the subspaces. Results obtained using the 20 PCs are presented as the main results and figures.

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